Longitudinal white matter changes in Alzheimer's disease; a tractography-based analysis study

Soichiro Kitamura, Kuniaki Kiuchi, Toshiaki Taoka, Kazumichi Hashimoto, Shotaro Ueda, Fumihiko Yasuno, Masayuki Morikawa, Kimihiko Kichikawa, Toshifumi Kishimoto

Corresponding author: Soichiro Kitamura
Department of Psychiatry, Nara Medical University, 840 Shijo-cho, Kashihara, Nara 634-8522, Japan.
Email: kitaso@naramed-u.ac.jp
Tel: +81-744-22-3051 (extension 3461)
Fax: +81-744-22-3854

Co-authors:
Kuniaki Kiuchi
Department of Psychiatry, Nara Medical University, Kashihara, Japan.
Email: kuniaki@naramed-u.ac.jp

Toshiaki Taoka,
Department of Radiology, Nara Medical University, Kashihara, Japan.
Email: ttaoka@naramed-u.ac.jp

Kazumichi Hashimoto
Department of Psychiatry, Nara Medical University, Kashihara, Japan.
Email: hkaz@naramed-u.ac.jp

Shotaro Ueda
Department of Psychiatry, Nara Medical University, Kashihara, Japan.
Email: shotaro@naramed-u.ac.jp

Fumihiko Yasuno
Department of Psychiatry, Nara Medical University, Kashihara, Japan.
Email:yasunof@naramed-u.ac.jp

Masayuki Morikawa

Sakai City Mental Health Center, Sakai, Japan.

Department of Psychiatry, Nara Medical University, Kashihara, Japan.

Email: AV6M-MRKW@j.asahi-net.or.jp

Kimihiko Kichikawa

Department of Radiology, Nara Medical University, Kashihara, Japan.

Email: kkichika@naramed-u.ac.jp

Toshifumi Kishimoto

Department of Psychiatry, Nara Medical University, Kashihara, Japan.

Email:toshik@naramed-u.ac.jp

Abstract

Alzheimer's disease (AD) classically presents with gray matter atrophy, as well as feature significant white matter abnormalities. Previous evidence indicates the overall burden of these pathological changes continues to advance as the disease progresses. The aim of this study was to investigate whether pathological alterations of white matter tracts correlate with the course of AD disease progression. 35 AD patients and 29 normal controls were recruited to the study and administered baseline magnetic resonance diffusion tensor imaging (DTI) acquisition and a cognitive function assessment at the time of initial evaluation. Subjects were re-evaluated with secondary DTI scan and cognitive function assessment at intervals of about 1.5 years on average. For the DTI acquired scans, we calculated diffusion tensor parameters, fractional anisotropy (FA), apparent diffusion coefficient (ADC), radial diffusivity (DR), and axial diffusivity (DA) along with the uncinate fasciculus (UNC), the inferior longitudinal fasciculus (ILF), and the inferior occipitofrontal fasciculus (IOFF). Compared to baseline, a significant mean FA reduction of the bilateral UNC, as well as a significant mean DR increase of the left UNC, was evident in AD patients at follow-up. Compared with normal controls, AD patients exhibited significant diffusion parameter abnormalities in their UNC, ILF, and IOFF. Taken together, these results indicate that progressive pathological white matter alterations can be quantified using the DTI parameters utilized here and may prove to be a useful biological marker for monitoring the pathophysiological course of AD.

Keywords

Abbreviation

AD, Alzheimer's disease; MTL, medial temporal lobe; DTI, Diffusion tensor imaging; ROI, region of interest; VBA, voxel-based morphometric analysis; MRI, magnetic resonance imaging; UNC, uncinate fasciculus; ILF, inferior longitudinal fasciculus; IOFF, inferior occipitofrontal fasciculus; FA, fractional anisotropy; ADC, apparent diffusion coefficient; D_A , axial diffusivity; D_R, radial diffusivity; MMSE, Mini Mental State Examination; ADAS-Cog, Alzheimer's Disease

Assessment Scale-cognitive component-Japanese version; NINCDS-ADRDA, National Institute of Neurological and Communicative Disorders and Stroke and the Alzheimer's Disease and Related Disorders Association; TR, repetition time; TE, echo time; ANOVA, analysis of variance

1. Introduction

Alzheimer's disease (AD) is the most common cause of dementia, and the number of AD patients have been increasing in recent years. AD shows symptoms of memory impairment and disturbance in orientation in its early stage, and then shows further higher brain dysfunction, such as visuospatial disturbance and executive dysfunction with disease progression. AD shows brain atrophy with disease progression. In imaging studies of AD, it has been shown that the medial temporal lobe (MTL) structuresbecome atrophied in the early stage, and further atrophy progressively spreads to the neocortical regions. Although AD is considered to affect mainly the cortical gray matter, pathological changes are also observed in the white matter, such as the loss of axons and oligodendrocytes together with reactive astrocytosis (Kobayashi et al., 2002; Roth et al., 2005). The executive function is consequent on activating the interaction across the several cortical regions, and it is considered that white matter abnormalities are related to the various cognitive dysfunction (Delbeux et al., 2007; Fellgiebel et al., 2008; Bozzali et al., 2011). Therefore, the neural connectivities across brain regions are important to comprehend the pathophysiology of AD.

Diffusion tensor imaging (DTI) is based on evaluating the random motion of water molecules, and can noninvasively examine neural microstructural tissue organization. In region of interest (ROI) analysis, microstructural damage is shown in the frontal, temporal regions or in the hippocampus in AD (Chen et al., 2009; Duan et al., 2006; Hong et al., 2010). The voxel-based morphometric analysis (VBA) in AD is known to show abnormality in the medial temporal structure and the hippocampus (Di Paola et al., 2007; Rose et al., 2008). Furthermore, the tract-based analysis, which extracts the diffusion parameters along the reconstructed white matter bundles, shows microstructural damage in the uncinate fasciculus, cingulated fasciculus, and the corpus callosum (Kiuchi et al., 2009.; Nakata et al., 2008; Pievani et al., 2010; Yasmin et al., 2007). Also, AD is a progressive neurodegenerative disease and shows atrophic changes and various clinical symptoms with disease progression. Matsuda et al. reported that progressive medial temporal lobe atrophy in a 3 dimension-magnetic resonance imaging (MRI) follow-up study was investigated in AD patients (Matsuda et al., 2001). Taken together, the research on longitudinal white matter changes would be important to understand AD pathophysiology. However, to the

best of our knowledge, a follow-up DTI study for white matter changes in AD has not been conducted.

In this study, we followed AD patients from the early stage to the moderate, and investigated their longitudinal white matter changes with disease progression. In the course of AD, pathological neuronal change begins in the medial temporal regions such as enthorhinal cortex, hippocampus and parahippocampus, which subsequently spreads to the neocortical regions with temporal, parietal and frontal cortex (Braak et al., 1995). Thus, pathological alterations in AD occur in temporal regions of the brain. Therefore, in recent study, we investigated three major white matter bundles, the uncinate fasciculus (UNC), the inferior longitudinal fasciculus (ILF) and the inferior occipitofrontal fasciculus (IOFF). The UNC is considered to play an important role in memory and cognition (Highley et al., 2002), and the ILF and IOFF are related to executive functions such as emotional process, object cognition, verbal and visual memory and visuospatial cognition (Chanraud et al., 2010; Kiuchi et al., 2011; Kringelbach et al., 2005). We hypothesized that the disruption in major white matter bundles can cause memory impairment or high cognitive impairments, and the connectivity of white matter tracts is impaired with disease progression.

In this study, we employed tract-based analysis to examine microstructural white matter changes with several major tracts in AD patients. Tract based analysis assembles the local diffusion tensor data into tracts using scalar metrics, such as fractional anisotropy (FA) and apparent diffusion coefficient (ADC). Furthermore, the coordinates of the tensor matrix can be diagonalized to extract the three eigenvalues; λ_1, λ_2, and λ_3 derived from the main eigenvectors of diffusion elements. The combination of these eigenvalues defines diffusion parameters, the axial diffusivity (D_A), in parallel with axon fibers, and radial diffusivity (D_R), perpendicular to axon fibers (Basser et al., 1998; Song et al., 2002; Sun et al., 2005). Thus, tract-based analysis can evaluate the specific anatomical localization of a single tract and allow measurement throughout the length of the bundles.

2. Results

2.1 demographic data

The demographic and neuropsychological characteristics are shown in Table 1. No significant differences were noted in age and educational level between AD patients and normal controls. Between baseline and follow-up, AD patients showed significant decline in Mini Mental state Examination (MMSE) and Alzheimer's Disease Assessment Scale-cognitive component-Japanese version (ADAS-Cog.) scores ($p < 0.005$).

2.2 FA and ADC

Table 2 shows the FA and ADC values of the UNC, ILF and IOFF for all the groups. Among the AD patients, compared with baseline point, the significant mean FA reduction of the bilateral UNC was shown at follow-up point (right, $p < 0.05$; left, $p < 0.01$). In contrast, no other metrics were significant between baseline and follow-up point. Compared with the normal controls, we found the significant mean FA reduction of the bilateral UNC (right, $p < 0.001$; left, $p < 0.001$), and the significant mean ADC increase of the bilateral UNC (right, $p < 0.001$; left, $p < 0.01$) and the right IOFF ($p < 0.05$) at baseline point in AD patients. Furthermore, AD patients showed the significant mean FA reduction of the right ILF ($p < 0.01$) and the bilateral IOFF (right, $p < 0.05$; left, $p < 0.05$), and significant mean ADC increase of the right ILF ($p < 0.01$) and the right IOFF ($p < 0.05$) at follow-up point.

2.3 D_A and D_R

The mean D_A and D_R values of the UNC, ILF and IOFF for all groups are shown in Table 3. Among the AD patients, the significant mean D_R increase of the left UNC ($p < 0.05$) and the marginally significant mean D_R increase of the right UNC were shown at follow-up point rather than at baseline point. In contrast, no other metrics were significant between baseline and follow-up point. Compared with the normal controls, AD patients showed the significant mean D_R increase of the bilateral UNC (right, $p < 0.001$; left, $p < 0.001$) and the right IOFF ($p < 0.05$) at baseline point. Additionally, AD patients showed the significant mean D_R increase of the right ILF ($p < 0.01$) and the left IOFF ($p < 0.01$) with disease progression.

3. Discussion

The present study explored the white matter microstructural abnormalities in AD patients with disease progression using tractography-based analysis. To the best of our knowledge, this is the first study where AD patients were followed and assessed for longitudinal changes of their white matter bundles. In this study, we found mean FA reduction of the bilateral UNC in the course of clinical follow-up among AD patients. In addition, compared with normal controls, white matter microstructural changes in ILF and IOFF were observed in AD patients. Furthermore, examining the diffusivity, we found increase of mean radial diffusivity in the bilateral UNC with AD disease progression.

It is known that the UNC connects the orbitofrontal cortex in the frontal lobe and anterior part of the temporal lobe, and plays an important role in memory and cognition (Highley et al., 2002). There have been previous reports of abnormality of the UNC in AD (Taoka et al., 2006; Yasmin et al., 2008). Yasmin et al. reported that AD patients showed a significant FA reduction in the bilateral UNC compared with healthy controls using tract-specific analysis, and Taoka et.al found a significant FA reduction and ADC increase in AD rather than in normal controls using a tract of interest method (Taoka et al., 2006; Yasmin et al., 2008). These results were consistent with our present study. Furthermore, we followed the AD patients and found FA reduction of the UNC with disease progression. This is consistent with a previous study which reported that the FA value of the UNC was positively correlated with the MMSE score and negatively correlated with the ADAS-Cog score in AD with DTI analysis (Morikawa et al., 2010). In AD pathology, the pathophysiological change occurs in the early AD stage in the MTL, which includes the transentorhinal region, entorhinal cortex, and hippocampus, which subsequently spreads to the temporal, parietal and frontal cortex in the disease course (Braak et al., 1995). Thus, it is suggested that progressive disruption of the UNC fiber reflects the pathological change due to deterioration in AD which may underlie AD pathophysiology.

In contrast, we found that there was no significant FA reduction or ADC increase in the ILF and the IOFF between baseline and follow-up period. On the other hand, AD patients were found to have significant FA reduction or ADC increase in the ILF of the IOFF compared with normal controls. In previous studies, the diffusion abnormalities of the ILF or the IOFF in AD have been reported, which were consistent with our recent data (Cho et al., 2008; Fellgiebel et al., 2008; Stricker et al., 2008). The ILF connects the occipital lobe with the

anterior part of the temporal lobe, and anteriorly joins the UNC to relay information to the orbitofrontal cortex (Catani et al., 2003). Meanwhile, the IOFF connects the occipital, posterior temporal, and the orbitofrontal areas, and also contains fibers that connect the frontal lobe with the posterior part of the parietal and temporal lobes (Taoka et al., 2006). It has been suggested that the ILF and the IOFF are associated with object recognition, visual spatial processing, visual and verbal memory, and visual emotional process (Chanraud et al., 2010; Kiuchi et al., 2011; Kringelbach et al., 2005). In the course of AD, patients show symptoms of memory impairment and disorientation in the early phase, and consecutively show cognitive decline such as emotional, visuospatial disturbance and loss of executive function. In this study, we observed gradual FA decrease and ADC increase in the ILF and IOFF from normal controls to baseline and follow-up AD patients, which suggested that the progressive microstructural damages to the ILF and the IOFF might be associated with cognitive decline in AD pathology.

Considering the diffusion analysis, we found significant increase in radial diffusivity in UNC among the follow-up rather than baseline among AD patients. Therefore, it was shown to increase the radial diffusivity in ILF and IOFF in AD patients compared with normal controls. In this study, we identified greater increase of radial diffusivity than that of axial diffusivity with disease progression. The previous DTI studies in AD showed an increase of radial diffusivity (Huang et al., 2007; Salat et al., 2010). This is consistent with our recent examination. Salat et al. reported an increase of radial diffusivity in the medial temporal, occipital, and precuneus in DTI analysis. Moreover, Stricker et al. reported that an increase of radial diffusion reflects a loss of myelin integrity and neural demyelination (Stricker et al., 2008). Progressive white matter axonal demyelination underlies AD pathology, resulting in critical disturbances in neural condition, and thus severely damaging brain function (Roher et al., 2002). Taking these studies together, we considered that our data might reflect these white matter pathological changes in AD.

There are some limitations to the current study. The first limitation is the measurement protocol for diffusion tensor imaging. We applied a 6-axis diffusion encoding gradient, which is a small number for diffusion encoding (Jones et al., 2004). Because the AD subjects in this study had several problems in their cognitive functions, we needed to set shorter imaging time by using smaller number of diffusion encoding. Furthermore, there is a study which describes that

the number of diffusion encoding does not exert any significant effect of visualization of the optic radiation (Yamamoto et al., 2007). This is also the reason for the number of diffusion encoding gradients. The second limitation is that the DTI images were obtained using a 1.5-Tesla MRI system, relatively weak magnetic fields, and the number of participants was comparatively small. We considered that future studies should include a larger number of participants using higher-field MRI system. The third limitation is that the follow-up period among AD patients was incongruent. In this study, AD patients were followed between one and three years. However, in this study, cognitive function in each AD patient did not get worse with disease progression, from mild to moderate stage, and so we thought that there was not a remarkable cognitive fluctuation among follow up of the AD patients due to the incongruent follow up period. The fourth limitation is that AD patients in this study were administered choline esterase inhibitors, which might affect somewhat the diffusion measures. We would investigate it in our future analysis.

In conclusion, we examined the longitudinal evaluation of the microstructural white matter changes in AD patients with DTI tractography analysis. We found diffusion abnormalities in the major white matter bundles with disease progression, which may reflect white matter changes in AD pathology. Therefore, quantifying the histopathological changes to white matter may be a useful biological marker for monitoring AD.

4. Experimental procedures

4.1. Subjects

The subjects in this study were 35 AD patients (11 males and 24 females) with probable AD and age-matched 29 normal controls (12 males and 17 females), recruited from the Department of Psychiatry, Nara Medical University, Kashihara, Japan. Probable AD was diagnosed according to the National Institute of Neurological and Communicative Disorders and Stroke and the Alzheimer's Disease and Related Disorders Association (NINCDS-ADRDA) criteria (Mckhann et al., 1984). Among the AD patients, 26 took 5 mg of donepezil, 2 took 10 mg, and 7 patients took no donepezil medication. AD patients who underwent baseline MRI acquisition and cognitive function assessment at the time of initial evaluation, were clinically followed up, and

underwent secondary evaluation at intervals of about 1.5 years on average. Assessment of cognitive function was examined according to a standardized cognitive battery of tests, including the MMSE and the ADAS-Cog., the reliability and validity of which have previously been confirmed in Japan (Homma et al., 1992). All participants were screened for comorbid medical and psychiatric conditions by means of clinical, physical, and neurological examinations. A somatic and neurological evaluation was undertaken in all subjects, with a routine laboratory examination and brain structural MRI. Exclusion criteria for all of the subjects were: a history of substantial head injury, seizures, neurological diseases, impaired thyroid function, and corticosteroid use. Subjects with cortical infarctions on T-2 weighted images were also excluded, whereas subjects with small lacunae in the white matter (fewer than 5 lesions on T2-weighted images) were included. Normal controls were people who had a medical examination and cognitive assessment including the MMSE at Nara Medical University hospital, and we excluded those who met the criteria for probable AD or DSM-IV axis I disorder. All subjects were right handed.

4.2. MRI acquisition

A 1.5-Tesla clinical MRI unit (Magnetom Sonata, Siemens AG, Erlangen, Germany) was used to obtain diffusion tensor images. Diffusion-weighted images were obtained using an echo planner imaging sequence (repetition time (TR) = 4900 ms, echo time (TE) = 85 ms, b = 1000 s/mm^2, 6-axis encoding, field of view = 230 mm, matrix = 128 x 128, slice thickness 3 mm with no gap, averaging = 6). We obtained 39 to 50 continuous slice images, covering the whole brain. We also acquired regular structural T1-weighted (spine-echo TR = 500, TE = 20) and T2-weighted (turbo spine-echo TR = 4000, TE = 110) images.

4.3. Image analysis

Tractographies were created using Volume One and dTV II DTI softwares developed by Masutani et al. (Masutani et al., 2003) (University of Tokyo, Diffusion Tensor Visualizer ver. 2; available at (http://www.ut-radiology.umin.jp/people/masutani/dTV.htm). Interpolation along the z-axis was performed to obtain isotropic data (voxel size, 0.89 × 0.89 × 0.89 mm). The eigenvector associated with the largest eigenvalue or the principal

axis was assumed to represent the local fiber direction. The tracking algorithm moved along the principal axis. The diffusion tensor at the next location was determined from the adjacent voxels, and its principal axis was subsequently estimated. Tracking lines were traced in this way, and propagated in both anterograde and retrograde directions until the FA fell below an assigned threshold. The settings for each tractography were as follows: the FA threshold for tracking was set at 0.18, the stop length was set at 160 steps and the seed and target ROIs are given in Table 4. Using these data, we delineated the bilateral UNC, ILF and IOFF (Figure). The dTV II software has a function that calculates the mean FA, mean ADC (10^{-3} s/mm^2), mean D_A (10^{-3} s/mm^2) and mean D_R (10^{-3} s/mm^2) along the constructed tract. We measured them along each tractography.

4.4. Statistical analysis

Data were analyzed using the Statistical Package for Social Science (SPSS for Windows 16.0; SPSS, Chicago, Illinois). Statistical analyses were performed on FA, ADC, D_A and D_R values by one-way analysis of variance (ANOVA) with follow up post hoc Bonferroni test.

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Figure legend

Figure
Tractography of the (a) uncinate fasciculus (UNC), (b) inferior longitudinal fasciculus (ILF) and (c) inferior occipitofrontal fasciculus (IOFF). The light blue colored object indicates the seed ROI, and the pink one does the target ROI. S; superior, I; inferior, A; anterior, R; right.

Table 1

Demograpchic and clinical data of the Alzherimer's disease patients and normal controls.

	AD		NC	p
	Baseline	Follow		
Number	35 (11/24)	35 (11/24)	29 (12/17)	
Age, mean (SD), y	75.3 (4.74)		73.3 (9.37)	N.S.
Education, meanSD)	11.7 (2.05)		11.5 (2.36)	N.S.
MMSE, mean (SD)	22.1 (2.28)	19.1 (3.20)	27.9 (2.13)	< 0.001
ADAS, mean (SD)	15.7 (5.77)	20.8 (7.42)		0.002

MMSE, Mini Mental State Examination; ADAS, Alzheimer's disease assessment scale cognitive subscale; NC, normal controls; AD, Alzheimer's disease; N.S., not significan

Table 2
The mean FA and ADC of the UNC, ILF and IOFF, and statistical analysis among all the groups.

Variable	Group			One - way ANOVA		Post-hoc Bonferroni T tet, p value		
	AD Baseline	AD Follow	NC	F	p value	AD Baseline vs. AD Follow	AD Baseline vs. NC	AD Follow vs. NC
UNC								
FA, R, mean (SD)	0.371 (0.101)	0.359 (0.023)	0.394 (0.018)	32.2	<0.001	0.013*	<0.001***	<0.001***
L, mean (SD)	0.367 (0.015)	0.351 (0.026)	0.397 (0.021)	37.6	<0.001	0.005**	<0.001***	<0.001***
ADC, R, mean(SD)	0.429 (0.017)	0.437 (0.025)	0.410 (0.016)	14.5	<0.001	N.S.	0.001**	<0.001***
L, mean(SD)	0.431 (0.021)	0.439 (0.024)	0.411 (0.014)	15.7	0.001	N.S.	<0.001***	<0.001***
ILF								
FA, R, mean (SD)	0.420 (0.021)	0.416 (0.016)	0.431 (0.023)	4.82	0.01	N.S.	0.086	0.009**
L, mean (SD)	0.428 (0.021)	0.423 (0.022)	0.432 (0.024)	1.37	0.259	N.S.	N.S.	N.S.
ADC, R, mean(SD)	0.433 (0.021)	0.439 (0.025)	0.422 (0.019)	4.92	0.009	N.S.	N.S.	0.007**
L, mean(SD)	0.440 (0.025)	0.445 (0.028)	0.433 (0.025)	1.689	0.191	N.S.	N.S.	N.S.
IOFF								
FA, R, mean (SD)	0.448 (0.021)	0.446 (0.021)	0.461 (0.022)	4.29	0.016	N.S.	0.066	0.021*
L, mean (SD)	0.451 (0.022)	0.447 (0.024)	0.463 (0.025)	3.93	0.023	N.S.	N.S.	0.02*
ADC, R, mean(SD)	0.431 (0.022)	0.432 (0.025)	0.417 (0.019)	4.53	0.013	N.S.	0.036*	0.023*
L, mean(SD)	0.432 (0.023)	0.438 (0.031)	0.424 (0.022)	2.45	0.092	N.S.	N.S.	0.088

UNC, uncinate fasciculus; ILF, inferior longitudinal fasciculus; IOFF, inferior occipitofrontal fasciculus; FA, fractional anisotrophy; ADC, apparent diffusion coefficient; R, right; L, left; N.S, no significant difference among the group; AD, Alzheimer's disease; NC, normal controls; ANOVA, analysis of variance $*p < 0.05$, $**p < 0.01$, $***p < 0.001$

Table 3

The mean axial and radial diffusivity of the UNC, ILF and IOFF, and statistical analysis among all the groups.

Variable	Group			One - way ANOVA		Post-hoc Bonferroni Tset, p value		
	AD Baseline	AD Follow	NC	F	p value	AD Baseline vs. AD Follow	AD Baseline vs. NC	AD Follow vs. NC
UNC								
Axial, R, mean (SD)	0.608 (0.022)	0.613 (0.029)	0.597 (0.019)	3.59	0.031	N.S.	N.S.	0.029*
L, mean (SD)	0.609 (0.027)	0.611 (0.034)	0.596 (0.019)	2.6	0.079	N.S.	N.S.	N.S.
Radial, R, mean(SD)	0.341 (0.015)	0.351 (0.022)	0.322 (0.015)	20.9	<0.001***	0.053	<0.001***	<0.001***
L, mean(SD)	0.345 (0.016)	0.355 (0.020)	0.321 (0.015)	32.8	<0.001***	0.048*	<0.001***	<0.001***
ILF								
Axial, R, mean (SD)	0.643 (0.026)	0.648 (0.033)	0.633 (0.021)	2.52	0.086	N.S.	N.S.	N.S.
L, mean (SD)	0.659 (0.035)	0.663 (0.035)	0.651 (0.031)	1.01	0.367	N.S.	N.S.	N.S.
Radial, R, mean(SD)	0.332 (0.021)	0.336 (0.023)	0.320 (0.019)	5.14	0.008	N.S.	0.076	0.007**
L, mean(SD)	0.331 (0.024)	0.341 (0.025)	0.327 (0.026)	2.77	0.068	N.S.	N.S.	N.S.
IOFF								
Axial, R, mean (SD)	0.659 (0.026)	0.658 (0.027)	0.648 (0.021)	1.72	0.184	N.S.	N.S.	N.S.
L, mean (SD)	0.662 (0.029)	0.665 (0.043)	0.657 (0.028)	0.49	0.616	N.S.	N.S.	N.S.
Radial, R, mean(SD)	0.322 (0.021)	0.323 (0.028)	0.305 (0.011)	5.83	0.004	N.S.	0.015*	0.007**
L, mean(SD)	0.320 (0.021)	0.328 (0.026)	0.390 (0.022)	5.34	0.006	N.S.	N.S.	0.005**

UNC, uncinate fasciculus; ILF, inferior longitudinal fasciculus; IOFF, inferior occipitofrontal fasciculus; R, right; L, left; AD, Alzheimer's disease; NC, normal controls; ANOVA, analysis of variance; N.S, no significant difference among the groups $*p < 0.05$, $**p < 0.01$, $***p < 0.001$

Table4
Definitions of the seed and target regions of interest for each tractography.

	Seed	Target
UNC	in the white matter of the frontal lobe on a coronal plane at the tip of the frontal horn of the lateral ventricle	in the white matter on a coronal plane at the tip of the inferior horn of the lateral ventricle in the ipsilateral temporal tip
ILF	in the white matter on a coronal plane at the tip of the inferior horn of the lateral ventricle in the temporal tip	in the ipsilateral sagittal stratum on a coronal plane at the level of the trigone of the lateral ventricle
IOFF	in the white matter of the frontal lobe on a coronal plane at the tip of the frontal horn of the lateral ventricle	in the ipsilateral sagittal stratum on a coronal plane at the level of the trigone of the lateral ventricle

UNC, uncinate fasciculus; ILF, inferior longitudinal fasciculus; IOFF, inferior occipitofrontal fasciculus.

seed ROI   target ROI   tracking line